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# Synchrotron Radiation in Medical Sciences

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# Synchrotron Radiation in Medical Sciences

## Growth and Outlook for an Emerging Field of Science



115 Years  
Later

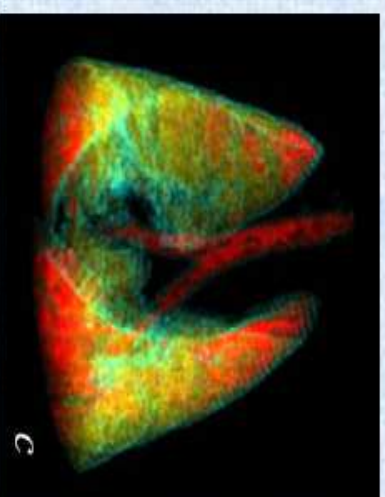


Wilhelm Roentgen's Laboratory  
University of Wurtzburg 1895

European Synchrotron Radiation Facility  
Grenoble France, 2010



Frau Roentgen's Hand



3D monochromatic high-resolution  
dynamic digital imaging

## Outline

- **Accelerators For Medical Applications**
- **Advantages of using SR for medical applications**
- **SR X-rays imaging techniques**
  - Absorption, K-edge and L-edge imaging
  - PHase Contrast Radiography (PHC)
  - Diffraction Enhanced Imaging (DEI)
- **Radiotherapy techniques with SR X-rays**
  - Microbeam Radiation Therapy (MRT)
  - Stereotactic Synchrotron Radiation Therapy (SSRT)
- **Medical Beamlines in Other Facilities**

# ACCELERATORS FOR MEDICAL APPLICATIONS

- More than **half** of particle accelerators at present running in the world are devoted to **medical applications**.
- The main areas of use are: (i) radioisotope production, (ii) **radiotherapy**, (iii) **biomedical research**.



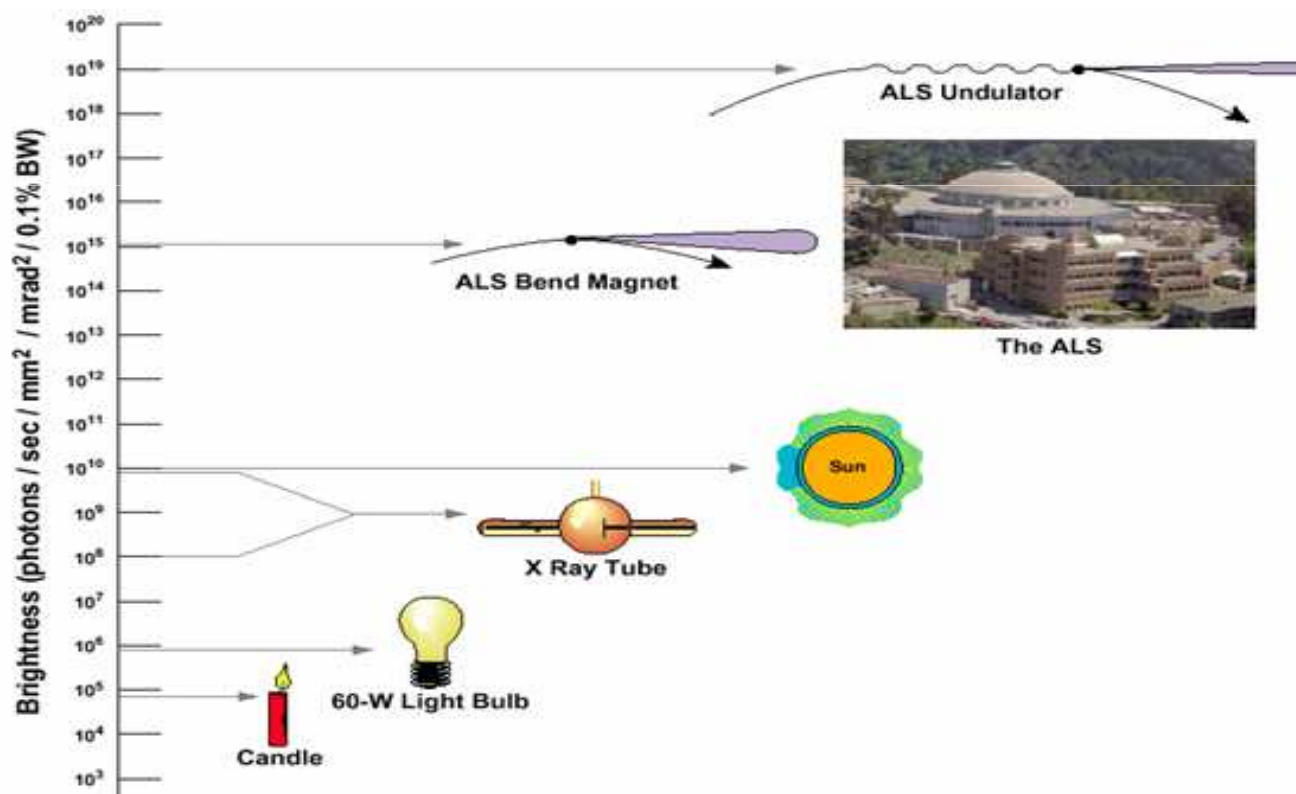
- **80%** of all the biomedical accelerators are devoted to **radiotherapy** with either X-rays or hadron beams.

## Cancer

- Worldwide the estimated number of new cancer cases each year is expected to rise from **10 millions** in 2000 to **15 millions** by 2020.
- Cancer is **second** cause of death in High-income countries and **third** in Iran
- Therefore **combating cancer** is a major societal and economical issue in the world

# Advantages of using SR for medical applications

**1. Brilliant** quick experiments on small samples, high dose-rates, reduction of exposure time



## Advantages of using SR for medical applications

- 2. Collimated** – the beam can be focused down to less than a micron, reduced scatter on images
- 3. Continuous spectrum** - from infrared to hard x-rays, optical devices select and scan
- 4. Polarised** – this minimises background scattering, improves sensitivity and enables measurement of circular dichroism
- 5. Pulsed** – the electron bunches produce nanosecond light pulses, enabling process kinetics to be followed and ‘movies’ of reactions to be made.

## Medical imaging with synchrotron radiation

- SR Medical imaging techniques are based on **absorption** and **refraction** of X-rays.
- **Phase effects** techniques require a high degree of spatial coherence of the radiation and it seems possible **only at SR facilities**.
- Excellent results is due to the **small opening angle** in the vertical direction and the possibility to place the detector at a **large distance**.
- **Beam hardening** due to the sample absorption of the low energy photons **is also avoided**.

## Phase detection imaging

- Conventional radiologic studies are based on only **absorption effects**.
- The effects on **propagation of the X-ray** wave can be described by the **refraction index  $n$** :  $n = 1 - \delta + i\beta$
- **imaginary component  $\beta$**  related to the **absorption** and by a **real component  $\alpha$**  related to **phase-shift** due to **scattering of the waves**.
- Phase contrast may also prove useful in biological and medical studies because it **falls off less quickly** at higher energies than absorption contrast:  $\delta \propto E^{-2}$ , whereas  $\beta \propto E^{-4}$ .
- **By increasing the energy**, phase contrast imaging could allow a **significant dose reduction** with little deterioration of the diagnostic information.

## phase contrast imaging

- Beyond the detail, the waves refracted (phase shifted) by the detail itself strongly **interfere** with the unrefracted waves.
- This interference effect takes place along the **border of the detail** inside a **narrow angular region** and it results in **strong interference patterns inside this region** that could be detected

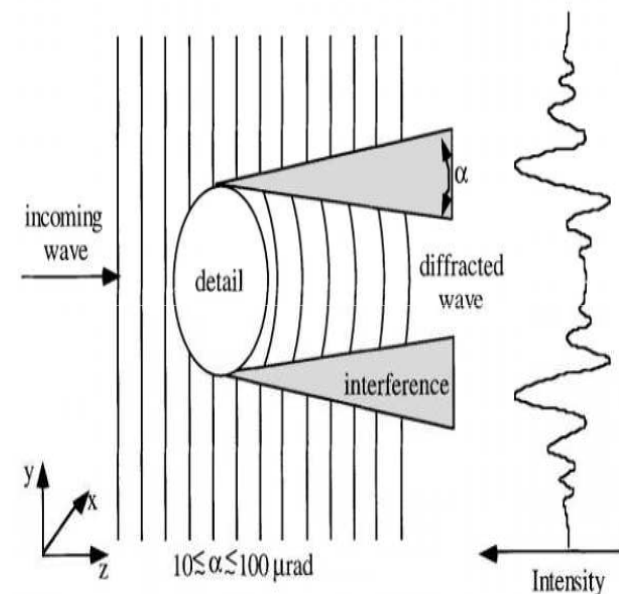
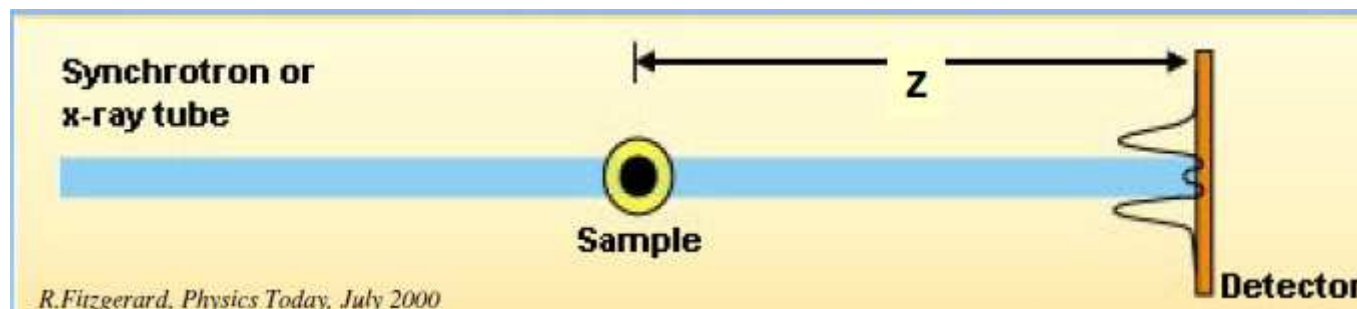
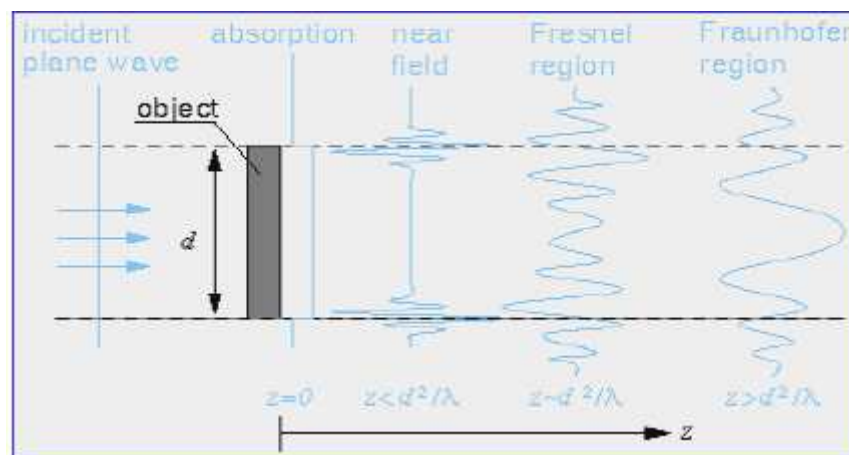


Figure 1.4: Scheme of the process that governs the in-line phase contrast technique.

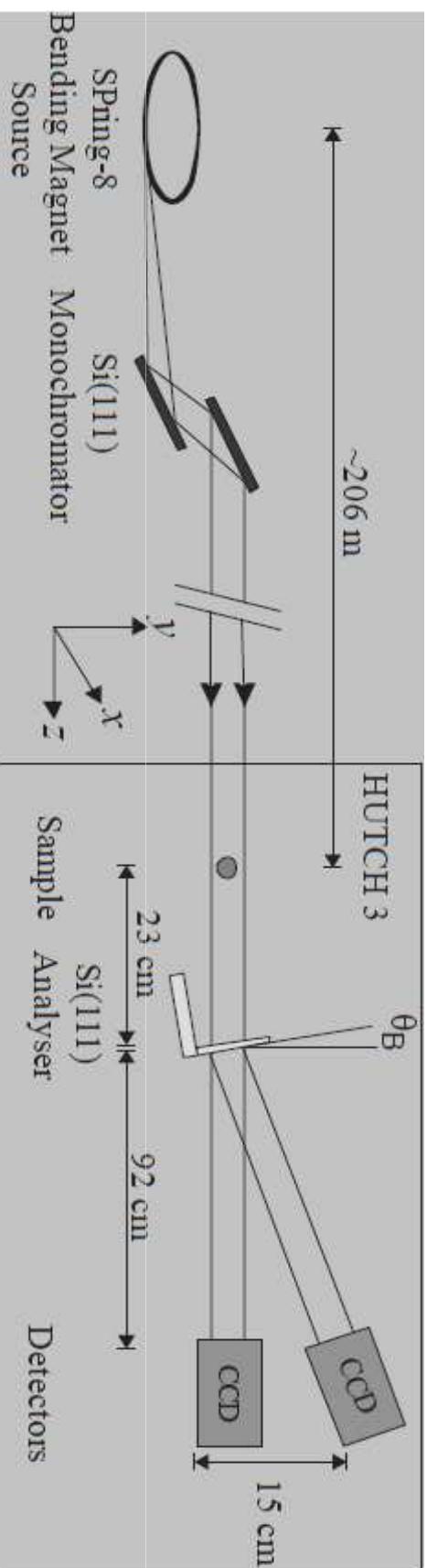
# PHase-Contrast radiography (PHC)



- The technique exploits the high spatial coherence of the X-ray source.
- $z = 0 \rightarrow$  absorption image
- For  $z > 0 \rightarrow$  interference between diffracted and un diffracted wave produces edge and contrast enhancement. A variation of  $\delta$  is detected

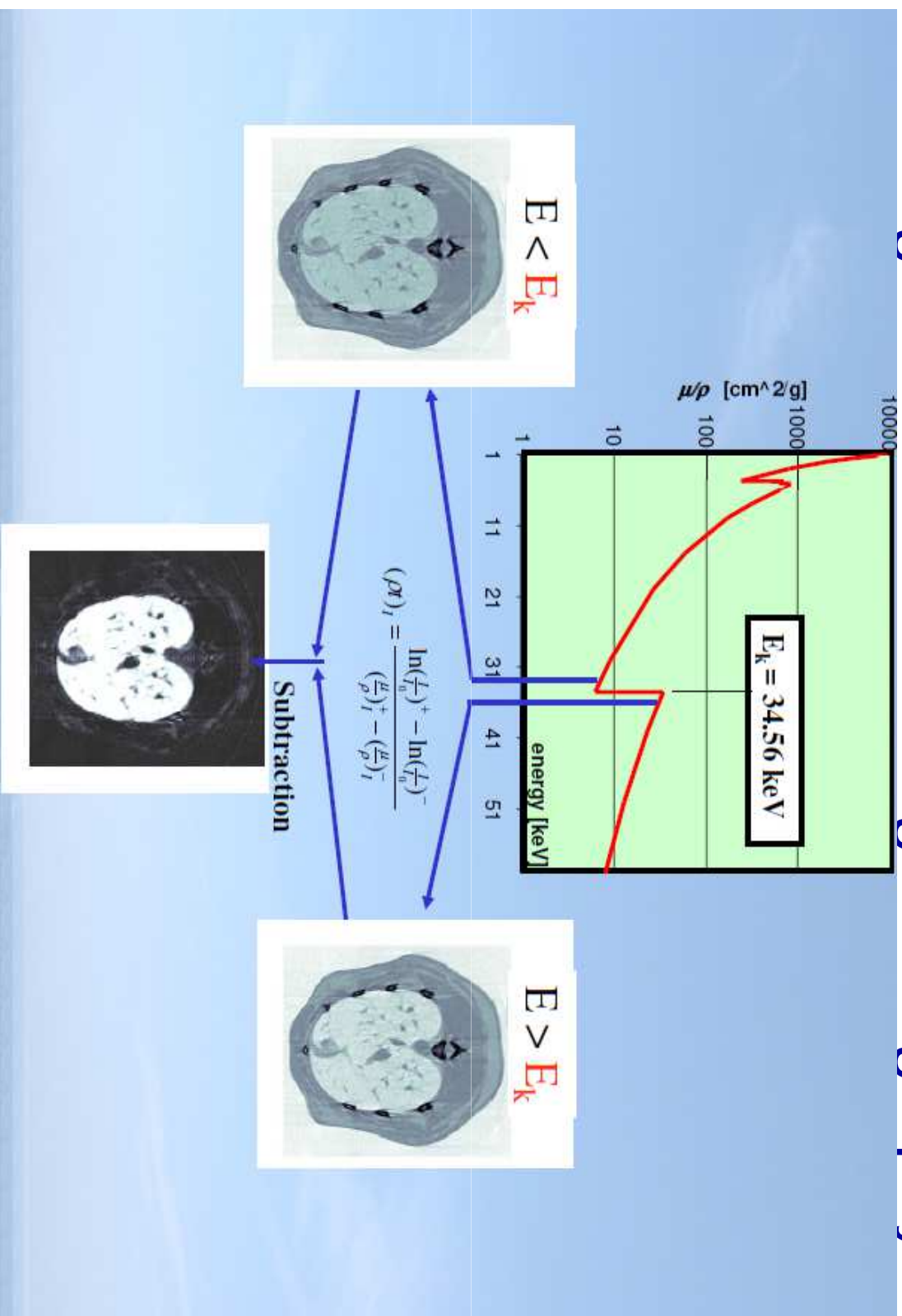


## Imaging Setup



- **Beamline 20B2, Spring-8, Japan. 25 keV beam of highly coherent radiation.**

# K-edge Subtraction Lung Tomography



Courtesy of A. Bravin (ESRF)

# Tomographic imaging at ESRF

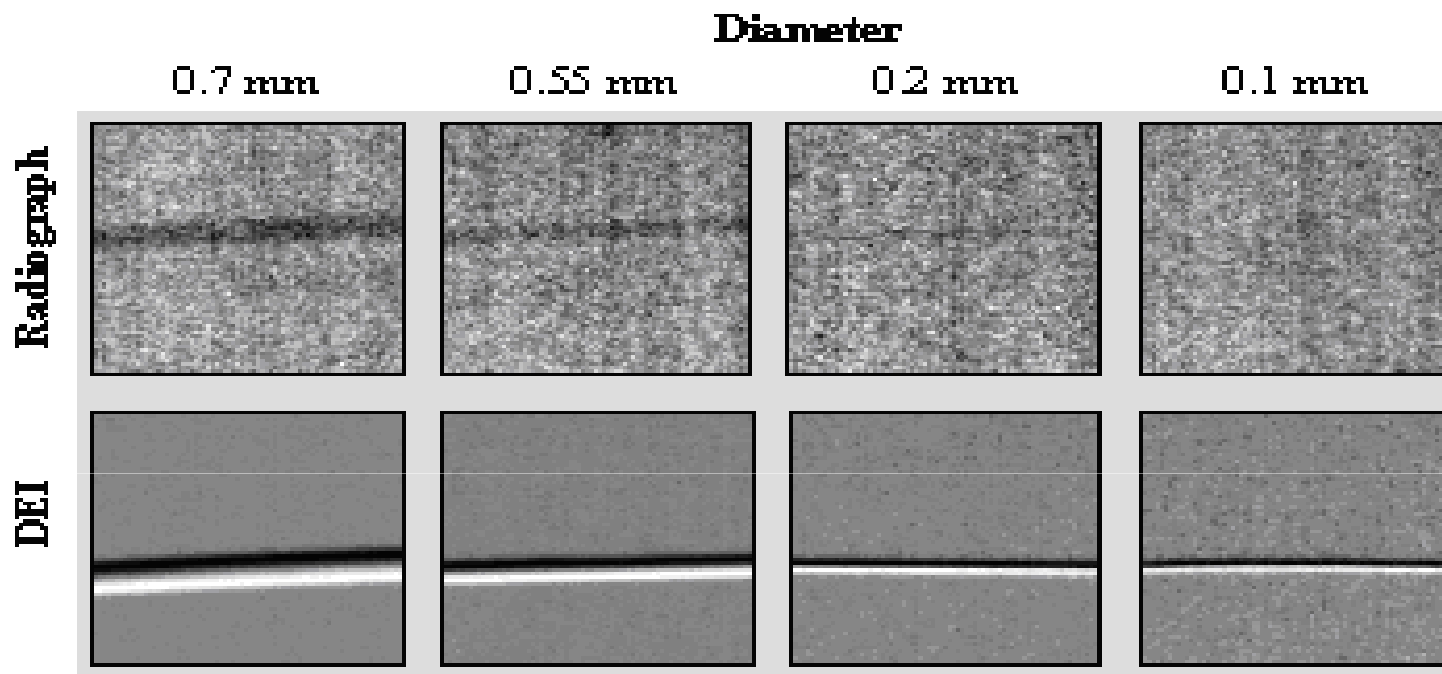


Courtesy of A.Bravin (ESRF)

## Applications

- Mammography
- Bronchography
- Musculoskeletal imaging
- Coronary angiography
- Micro-angiography
- Computed tomography
- Micro-tomography
- Cartilage and bone imaging

## Comparison



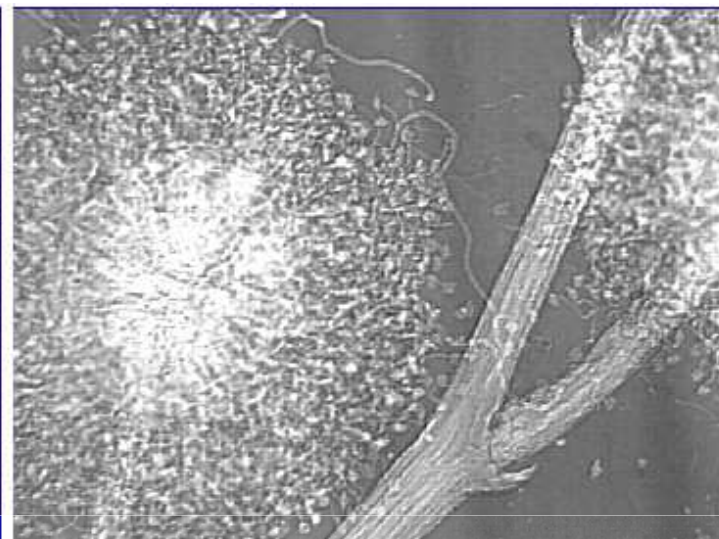
Conventional radiograph vs. DEI image of a nylon fiber. With conventional radiography, smaller objects show little contrast, a drawback that is not seen in the DEI images.

## Images of a Mimosa flower

25 keV

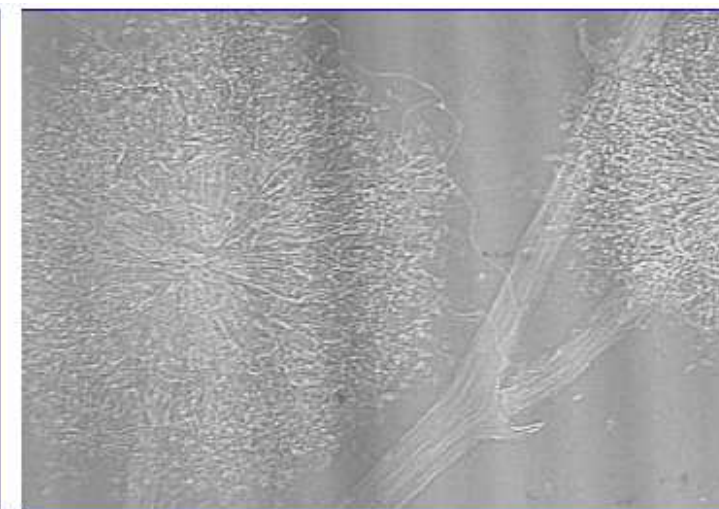
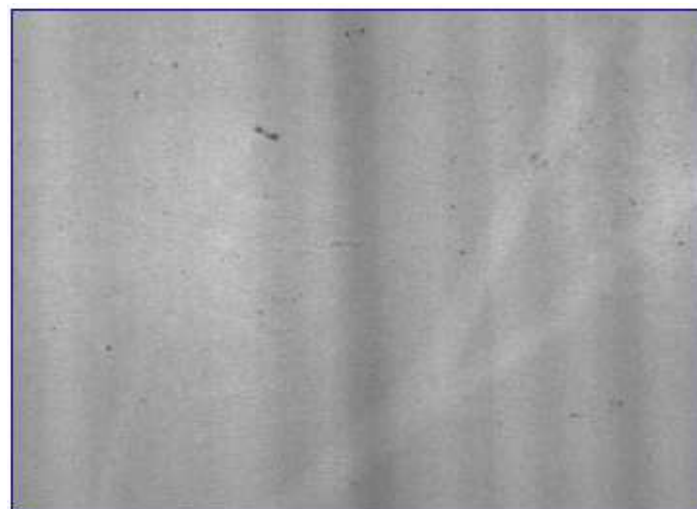


Absorption



Phase-contrast

10 keV



## X-ray imaging of the lung

Absorption Contrast



Phase Contrast, 25 keV,  $z=2$  m



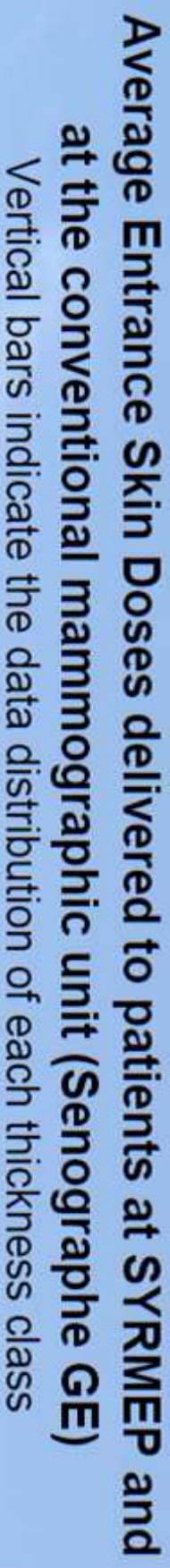
*Courtesy of Marcus Kitchen, School of Physics*

DEI

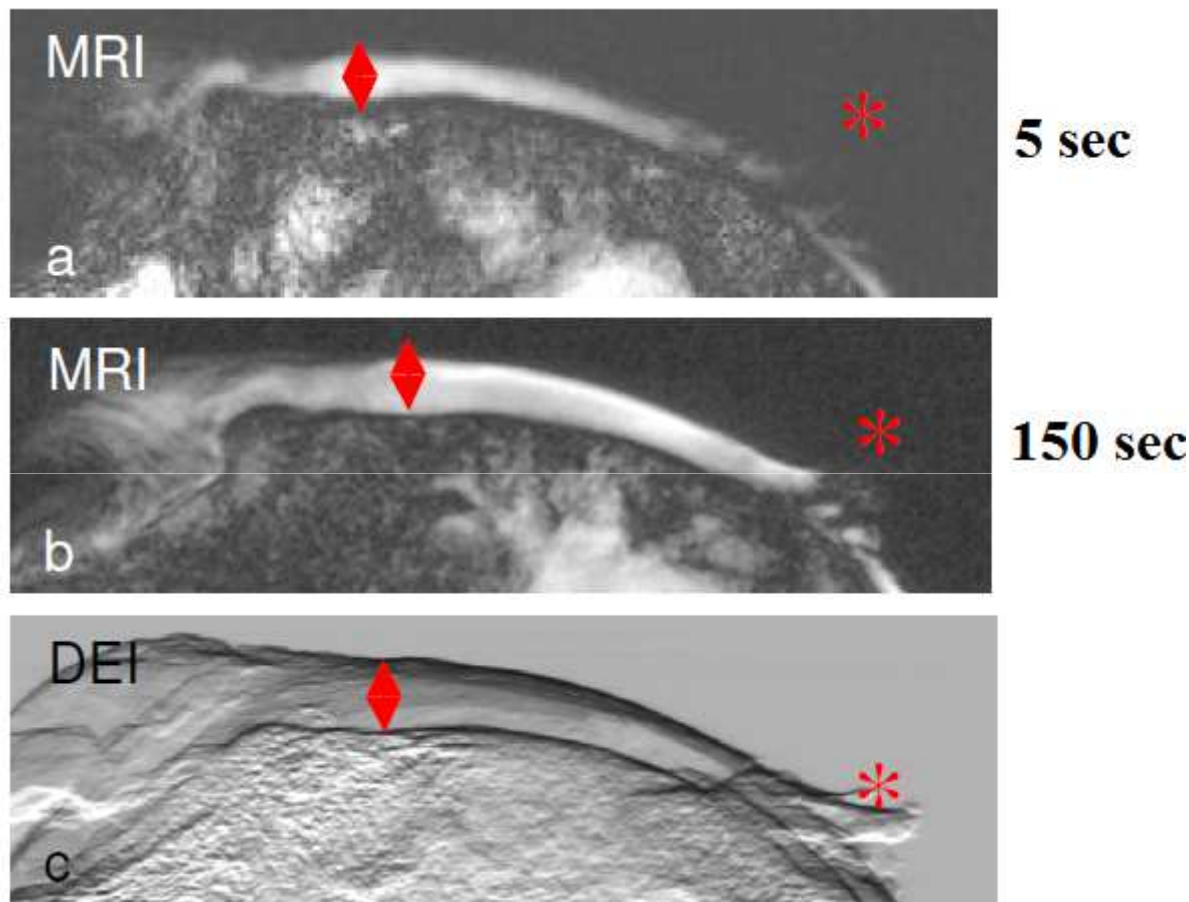


ILSF-IPM, Sep. 2013

### 3<sup>rd</sup> ILSF School on Synchrotron Radiation and Its Applications

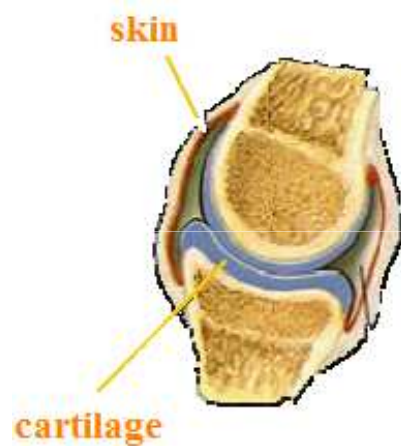


# Femur head core cuts: comparison with MRI



A Wagner, M Aurich, N Sieber, M Stoessel, WD Wetzel, K Schmuck , M Lohmann, B Reime, J Metge, P Coan, A Bravin, F Arfelli, L Rigon, RH Menk, G Heitner, T Irving, Z Zhong, C Muehleman, J A Mollenhauer submitted to NIM A

## DEI studies of the finger joint



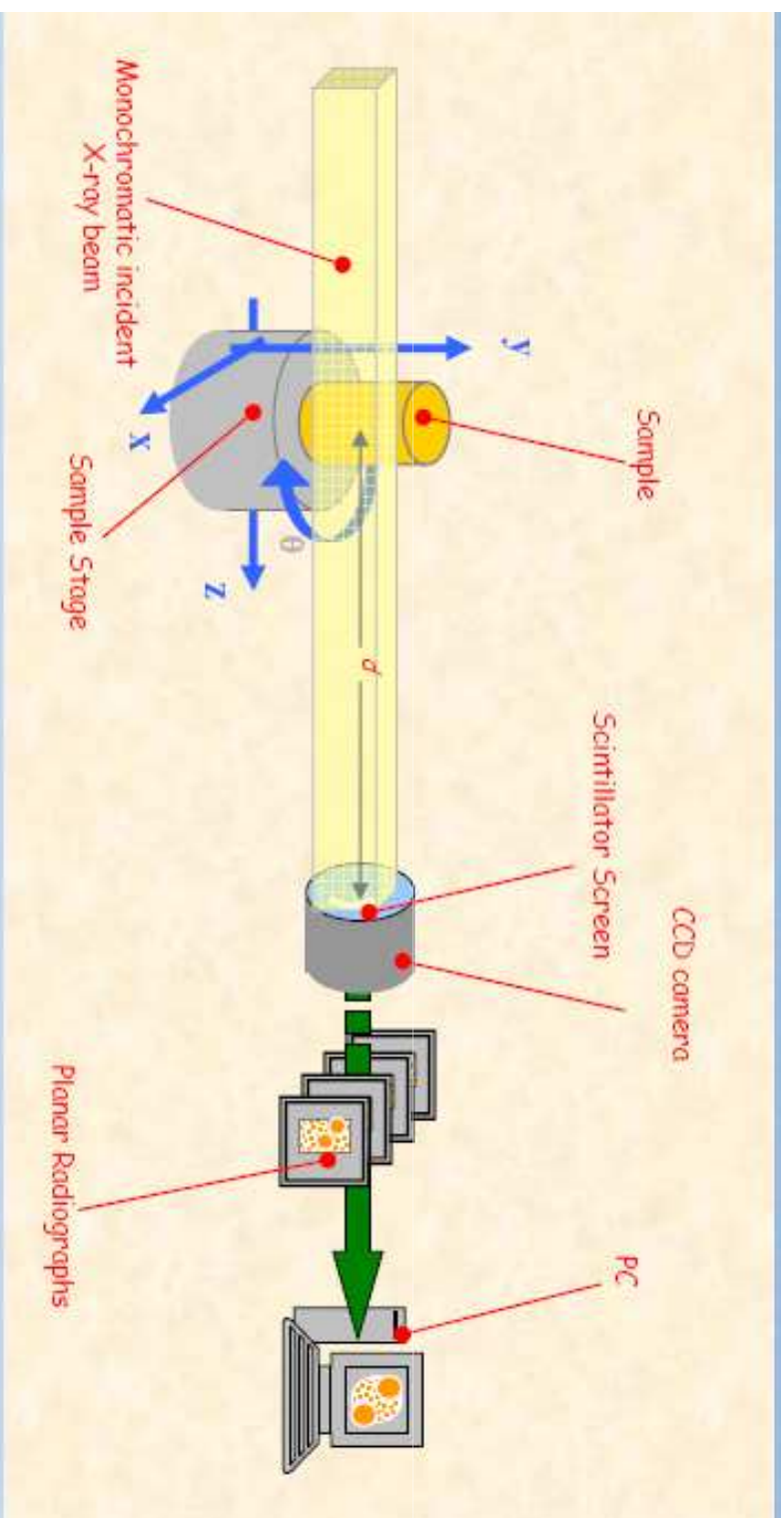
Conventional radiograph



Apparent absorption image @ 20keV  
at ELETTRA

*Daresbury, Elettra, University of Trieste Collaboration within PHASY project: R. Lewis et al.*

# Computed $\mu$ -Tomography ( $\mu$ -CT)



## Phase Contrast Imaging

■ Air bubbles in water. Pixel Size = 2.8  $\mu\text{m}$ , Energy=25 keV

400 $\mu\text{m}$

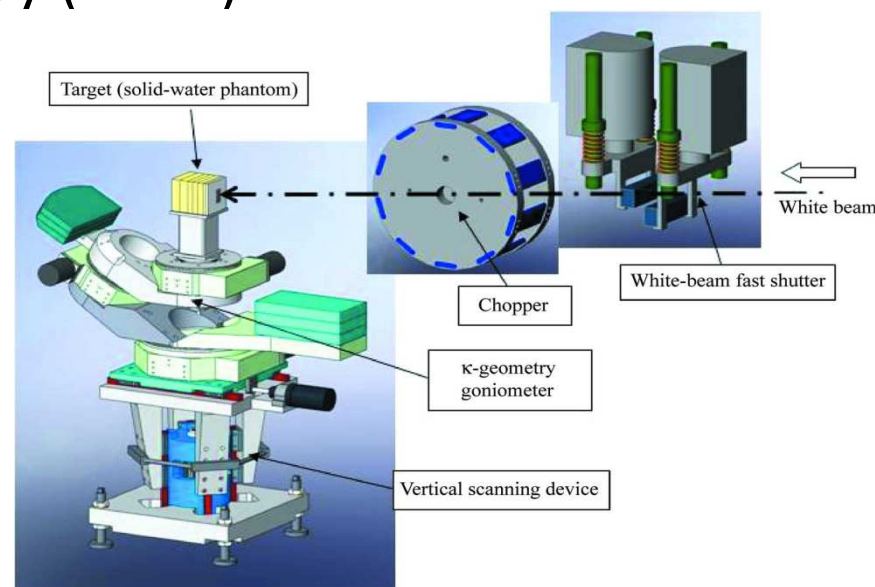
X-ray set:  $R_1=1.0\text{ m}$   
 Source fwhm:  $100\times100\mu\text{m}$

SP8 BL20B2:  $R_1=210.0\text{ m}$   
 Source fwhm:  $150\times10\mu\text{m}$

# Synchrotron Radiation Therapy

Modern technological radiotherapy techniques:

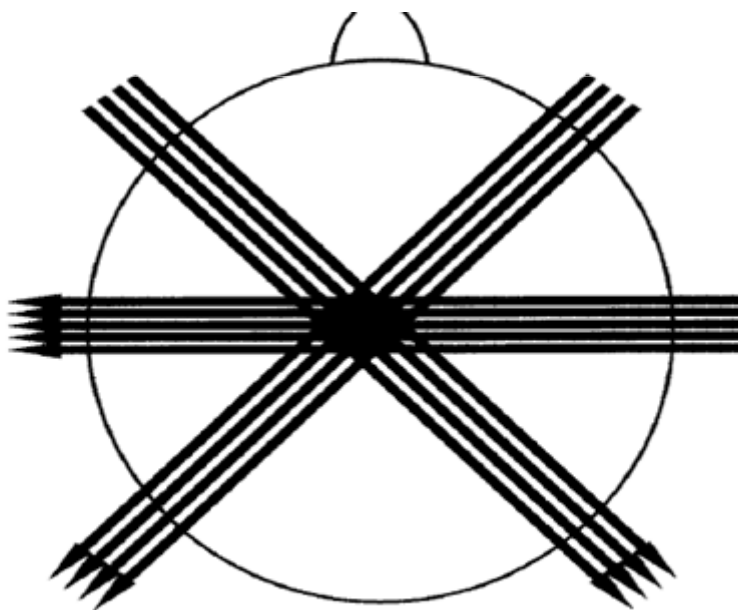
- 3-Dimensional **Conformal Radiotherapy**
- Intensity-Modulated Radiation Therapy (**IMRT**)
- Image-guided radiation therapy (**IGRT**)
- Boron Neutron Capture Therapy (**BNCT**)
- Ion Therapy
- Stereotactic Radiosurgery



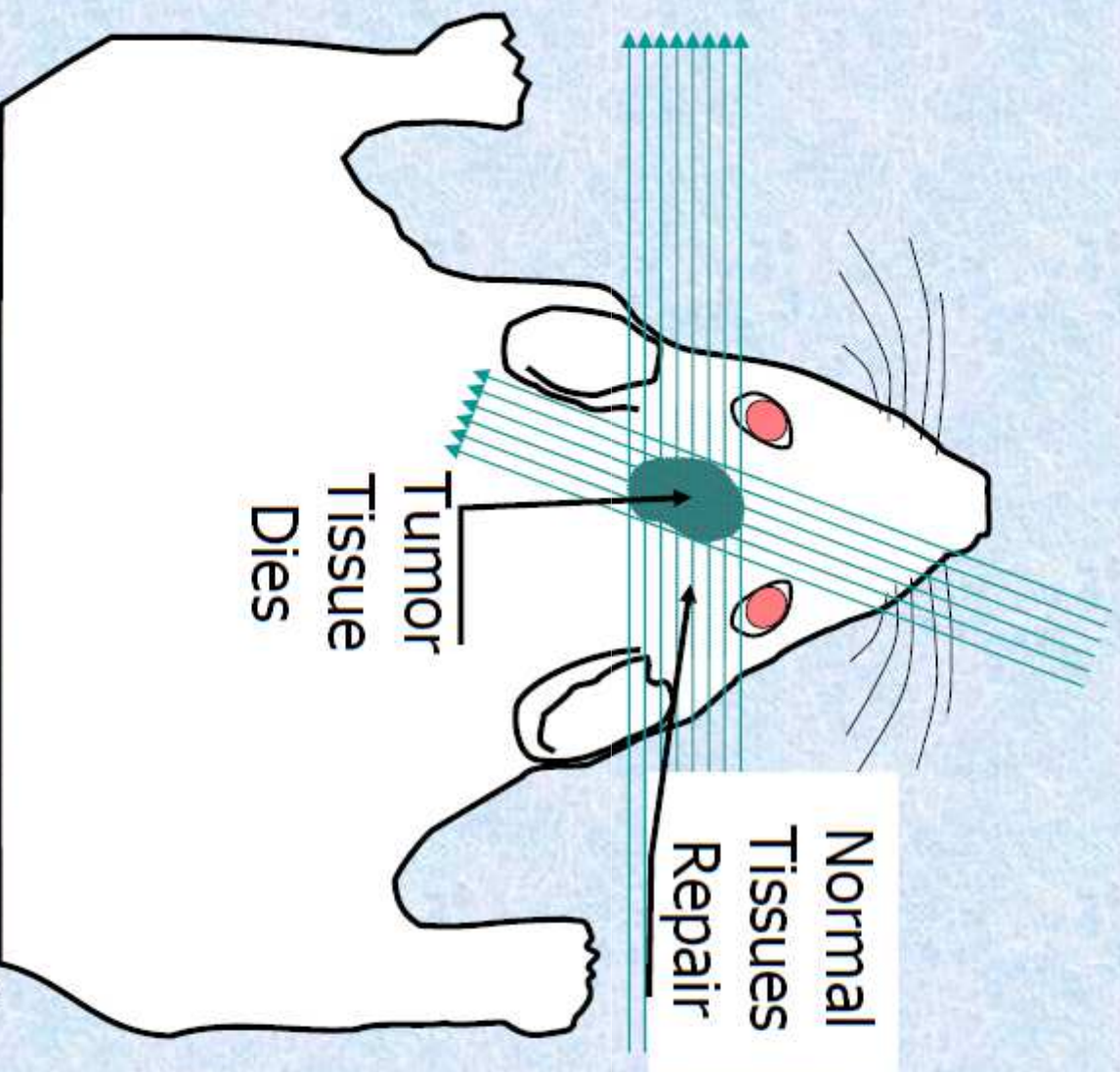
# Synchrotron Radiation Therapy

- It was Larsson (1983) who **first pointed** out the properties of synchrotron radiation that were desirable for radiotherapy.
- The inherent **high collimation** means that it can be targeted with great accuracy onto **small tumours** whilst the ability to **tune the energy** of a monochromatic beam means that the beam energy can be optimized for a particular depth.

In order to achieve this the beam is split by collimators into many smaller beams (microbeams), which are spatially separated but parallel. The typical thickness of each microbeam is 20–50  $\mu\text{m}$  with a separation of 100–200 m



# Bidirectional Irradiation (MRT)



# Microbeam Therapy

- High doses ( $>100$  Gy) are delivered in one fraction by using arrays of parallel thin beams. In MRT beam widths range from 25 to 100 mm, whereas in MBRT the beam width employed at the ESRF is 600 mm.
- MBRT might be a promising technique to treat brain tumors and some illness like epilepsy with no significant secondary effects.

## Microbeam Therapy

The main attributes of microbeams are:

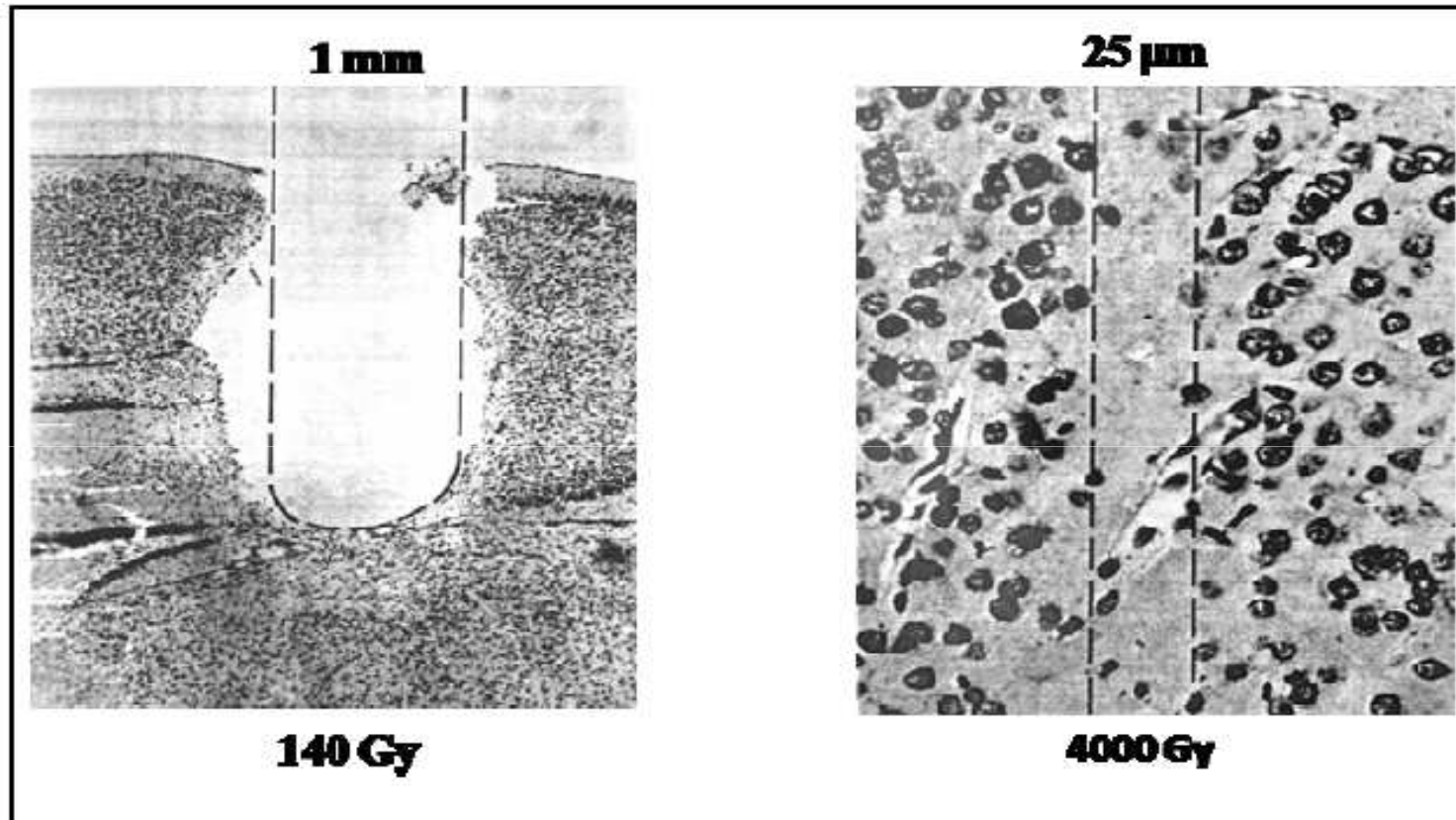
- (a) **Their sparing effect** on normal tissues, including the central nervous system (CNS).
- (b) **Their preferential damage** to tumors.

## Microbeam Therapy

Microbeam radiation therapy is aimed at clinical applications of:

- Pediatric brain tumors
- Tumors in the radio-sensitive organs such as those of the lower brain and spinal cord.

## Dose comparison



Histological images after irradiation using a millimetric beam (left) or a microbeam (right).

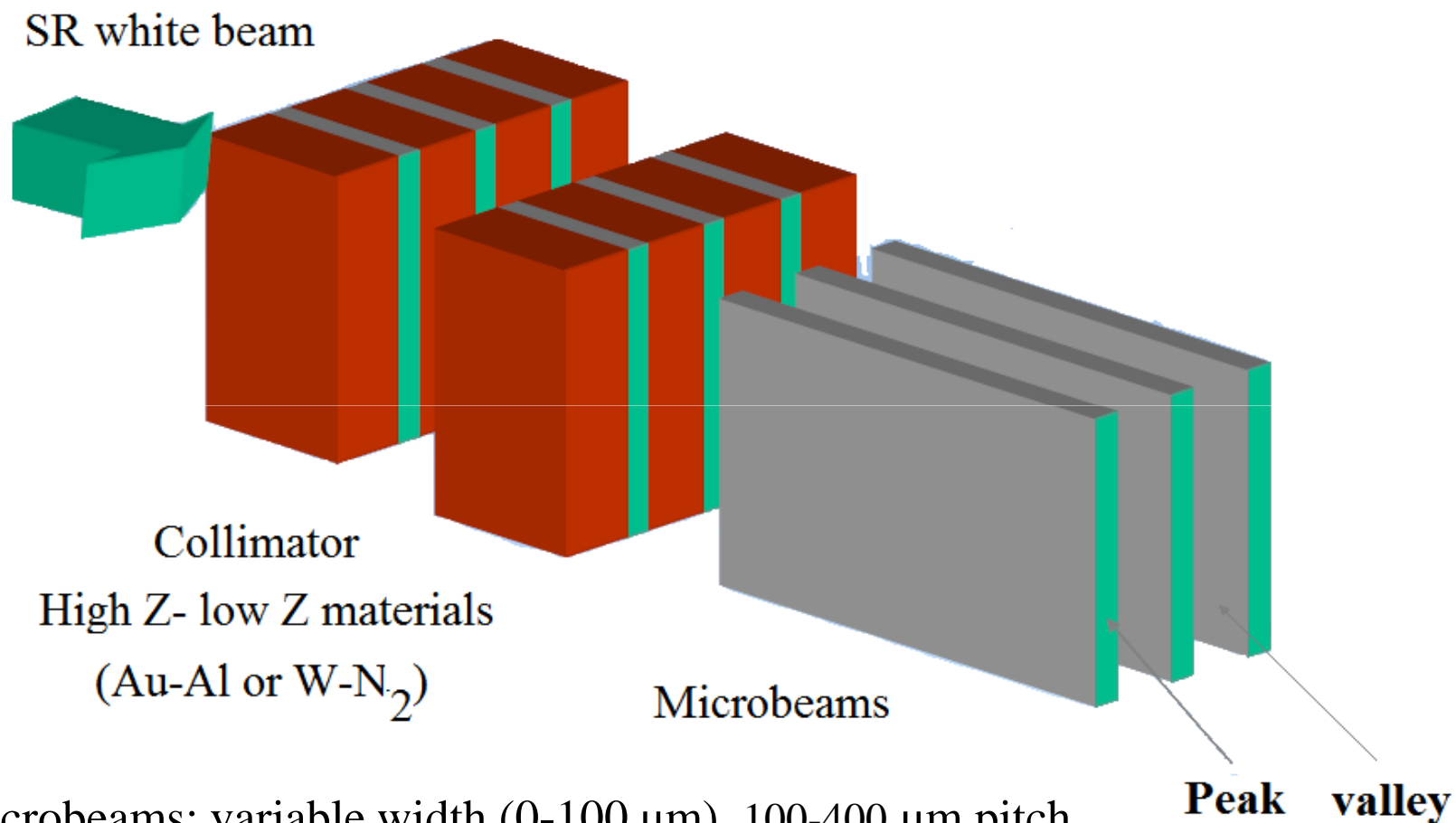
*Zeman et al., Radiat. Res. 15, 496,1961*

# Dose volume-effect

Beam diameter ( $\mu\text{m}$ )		Threshold dose (Gy)
25	CELLS	4000
75		500
250		360
1000	Tissues	140

(Fike & Gobbel, 2001)

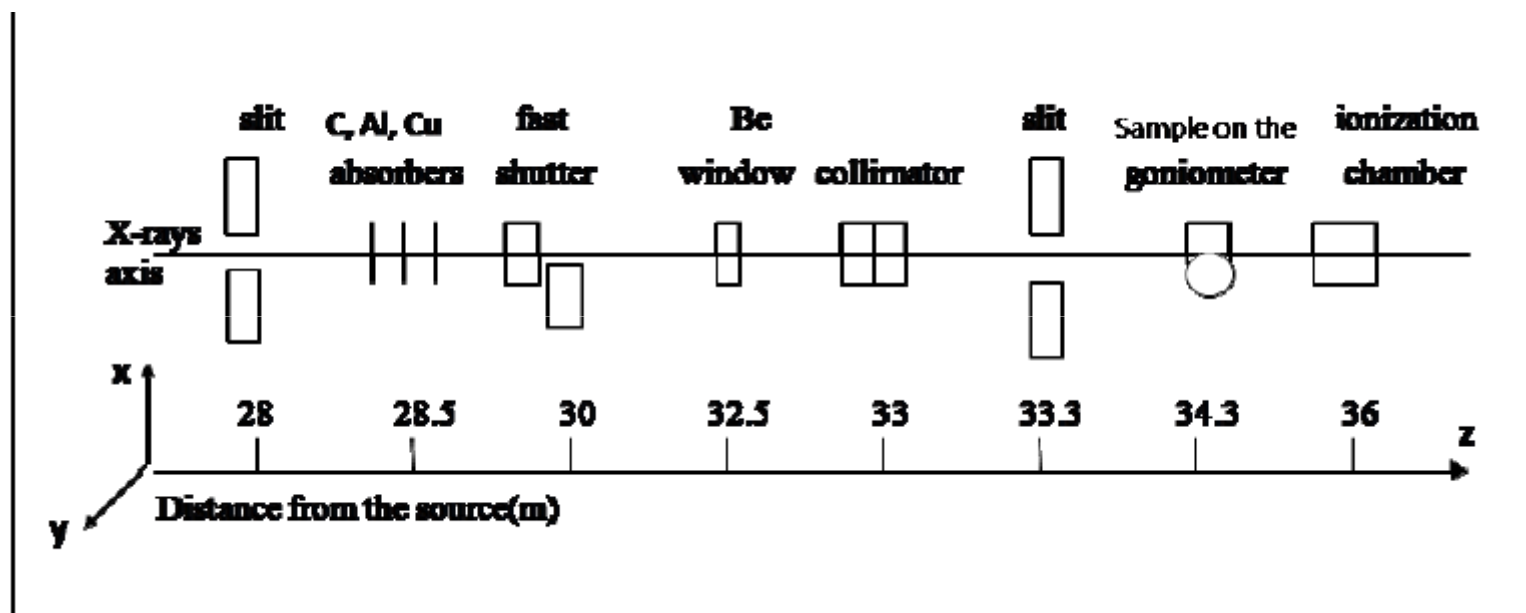
# Microbeams production



Microbeams: variable width (0-100  $\mu\text{m}$ ), 100-400  $\mu\text{m}$  pitch  
50-125 microbeam array to cover up to 5x5 cm<sup>2</sup>

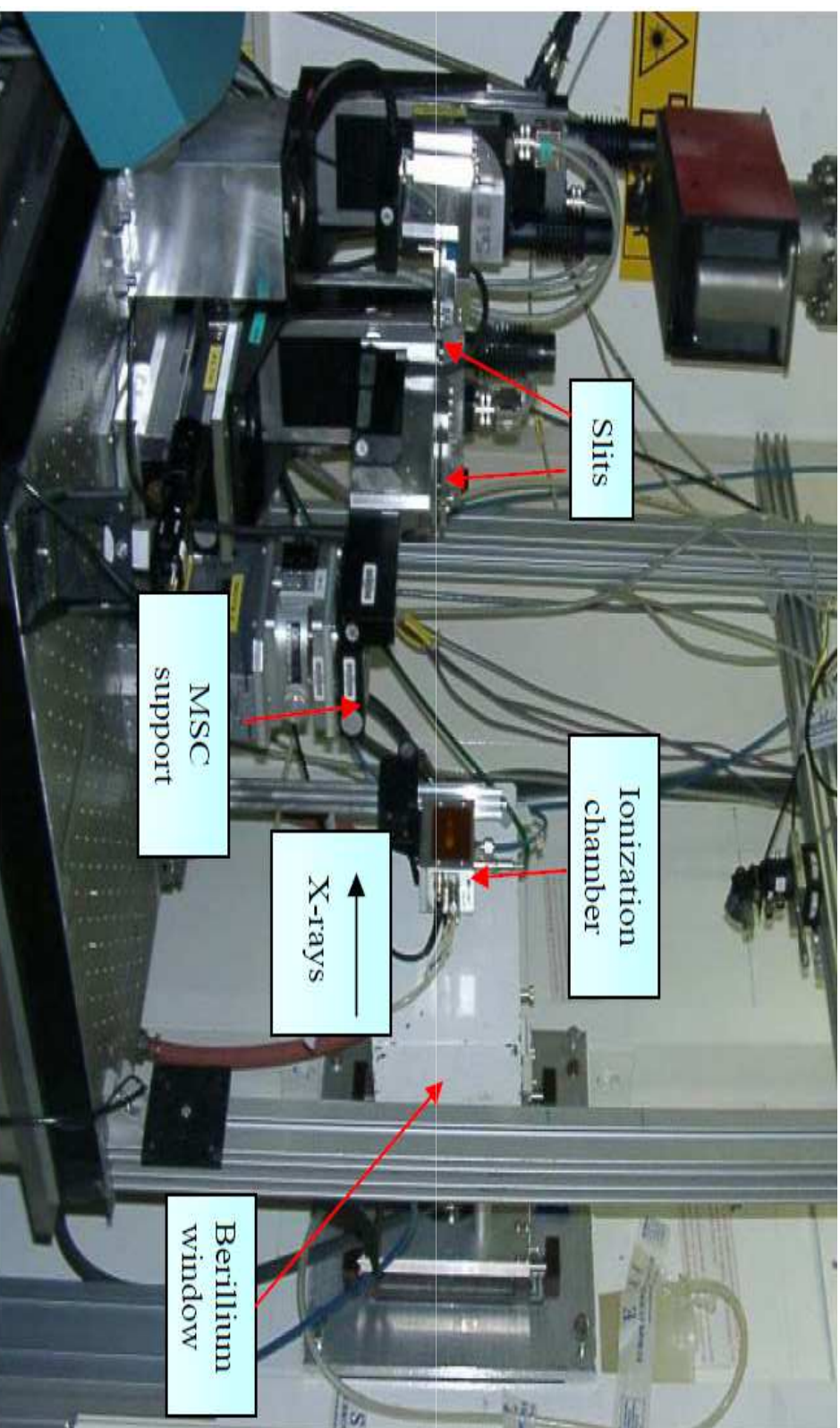
*Brauer et al. Rev.Sci.Instr.76, 064303, 2005*

## The experimental station for MRT



Schematic representation of the beamline setup for MRT, indicating the distance of each element from the light source.

## System setup

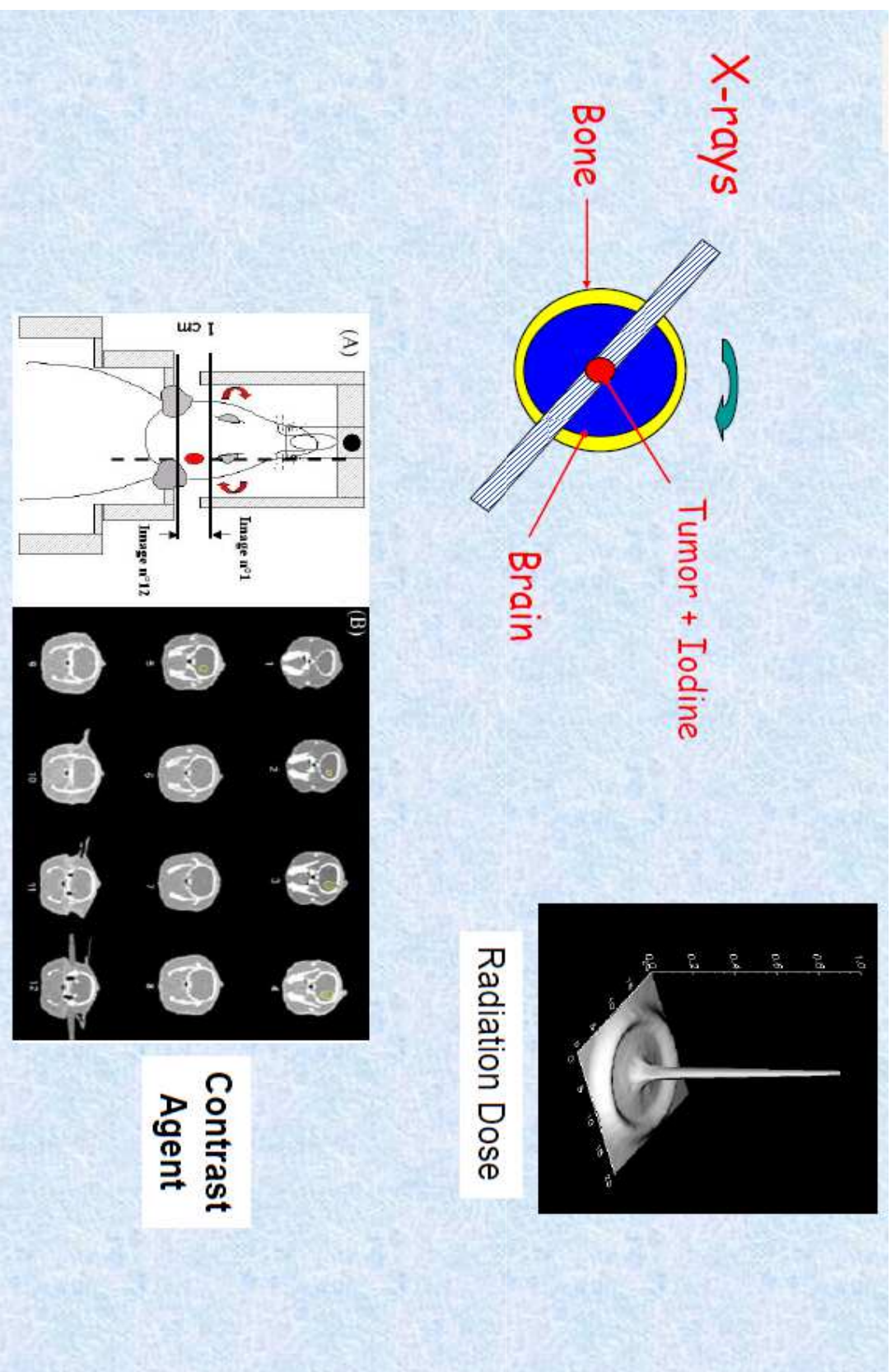


**Setup of the MRT experimental hutch (multislit collimator).**

## Photon Activation Therapy (PAT)

- PAT is an analogous method where a cascade of **Auger and photoelectrons** is created in the tumour during irradiation by a monochromatic SR beam.
- PAT is a **two-step** therapy, where a sufficient concentration of a **high-Z containing compound** is physiologically directed to the tumour.
- SR with an energy **slightly above the K-absorption** edge is targeted on the tumour, and the Auger electrons deposit their energy near the atom where photoabsorption takes place.
- Consequently, the heavy absorbing atoms should be incorporated as close to the DNA of the tumor cell as possible.

# Contrast Enhanced Stereotactic Radiotherapy



# Components

- Insertion device (bending magnet, wiggler, undulator)
- Front end (shieldings, filters, shutters, filters)
- Different hutches (imaging and therapy)
- Control room(s)
- Sample preparation laboratories
- Animal preparation room
- Cell laboratory
- Chemical laboratory

## Advantages vs Disadvantages

- Higher Quality of Images, Lower dose to patient, Higher contrast, Faster, Higher resolution, Capable of treatment of resistant tumors, Higher sensitivity (submicron)
- Preclinical (research) stage, Higher costs, Unknown, Not ease of access



گندم و جو کی پھل



*Thanks  
for  
your attention*